

1       **ELECTRONIC ENDOSCOPE APPARATUS ADAPTABLE TO ENDOSCOPES**  
2       **EQUIPPED WITH IMAGING DEVICE WITH DIFFERENT PIXEL DENSITY**

5                   **BACKGROUND OF THE INVENTION**

6       **[0001]**       This application claims the priority of Japanese  
7       Patent Applications No. 2001-1828 filed on January 9, 2001  
8       which is incorporated herein by reference.

10                   **Field of the Invention**

11       **[0002]**       The present invention relates to an electronic  
12       endoscope apparatus, specifically to a configuration of an  
13       electronic endoscope apparatus wherein electronic endoscopes  
14       having an imaging device with different pixel densities are  
15       connected to a common processor unit.

17                   **Description of the Prior Art**

18       **[0003]**       FIG. 3 shows the configuration of a part of a  
19       conventional electronic endoscope apparatus and, as shown in  
20       the figure, a CCD (Charge Coupled Device) 2, which is a  
21       solid-state imaging device, is disposed at the tip of an  
22       electronic endoscope 1. The endoscope 1 is configured to  
23       connect detachably to a processor unit 3, and the processor  
24       unit 3 is provided with a drive pulse generation unit 4 for  
25       generating drive pulses to drive the CCD 2 and a signal

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1 processing circuit 5 for performing various signal processing  
2 to form image signals (video signals) based on the output signal  
3 of the CCD 2. And the output of the signal processing circuit  
4 5 is supplied to a monitor 6.

5 [0004] According to the configuration described above,  
6 although not shown in the figure, light is emitted from the  
7 tip part, and the object to be observed is imaged with the  
8 CCD 2 under the emitted light and, at the CCD 2, electric charges  
9 accumulated in each pixel are read out as the image information  
10 by the drive pulse generation circuit 4. Thus the drive pulse  
11 generation circuit 4 generates various drive pulses such as  
12 a horizontal drive pulse, a vertical drive pulse, and a  
13 sweep-out (SUB) pulse, and these drive pulses are provided  
14 to the CCD 2 and thereby the image information constituting  
15 the video signal is read out.

16 [0005] The output signal of the foregoing CCD 2 is supplied  
17 to the signal processing circuit 5, where various image  
18 processing such as correlated double sampling, amplification,  
19 and gamma correction are performed and, from the signal  
20 processing circuit 5, video signals such as R (Red), G (Green),  
21 B (Blue) signals or Y (Luminance)/C (Color) signals are  
22 outputted to the monitor 6. Consequently, an observation  
23 image of the object to be observed is displayed in color.

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SUMMARY OF THE INVENTION

[0006] In the foregoing electronic endoscope apparatus, various types of electronic endoscopes 1, which have a built-in imaging device with different pixel densities as the CCD 2, are fabricated. For example, a endoscope with a reduced diameter, which utilizes a CCD 2 with fewer pixels than those of a conventional type, has been proposed, and there exists a endoscope with built-in CCDs 2 with different pixel densities to meet the need for higher resolution or to comply with different television standards. Since these CCDs 2 need to be driven by a drive signal which conforms to the pixel density of each CCD 2, the electronic endoscope 1 and the processor unit 3 in the configuration of FIG. 2 are designed in a single set corresponding to the pixel density of the CCD 2. Also, in the foregoing conventional drive pulse generation circuit 4, it is common practice to generate various drive signals in accordance with various conditions, such as the length of various electronic endoscopes 1, other than the foregoing pixel density.

[0007] However, fabricating a separate processor unit 3 to conform to each electronic endoscope 1 having a built-in CCD 2 with different pixel densities leads to unavoidable waste in terms of apparatus configuration or cost. Moreover, there is a problem in that there are limits in coping with the diversifying pixel density of CCD 2 when various requirements

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1 of different types of electronic endoscopes 1 need to be met  
2 by means of the foregoing drive pulse generation circuit.

3 [0008] Furthermore, there is proposed a type of apparatus  
4 of which electronic endoscope 1 comprises a drive pulse  
5 generation circuit which conforms to the pixel density of the  
6 CCD 2, and therefore there is a need for a processor unit to  
7 support both types of electronic endoscopes with and without  
8 the drive pulse generation circuit.

9 [0009] The present invention has been made in view of the  
10 above described problems, and its object is to provide an  
11 electronic endoscope apparatus which allows to conform to  
12 imaging devices with different pixel densities by use of a  
13 single processor unit, thereby avoiding any waste in terms  
14 of configuration or cost.

15 [0010] To achieve the above object, an embodiment of the  
16 invention according to claim 1 includes: a first endoscope  
17 having a first image device; a second endoscope having a second  
18 image device with a pixel density different from that of the  
19 foregoing first image device and having a second drive pulse  
20 generation circuit to generate a drive pulse to drive the second  
21 image device; and a processor unit for connecting the foregoing  
22 first or second endoscope, and is characterized in that the  
23 processor unit comprises: a first drive pulse generation  
24 circuit for generating a drive pulse to drive the foregoing  
25 first imaging device; a selection circuit for activating the

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second drive pulse generation circuit when the foregoing second endoscope is connected; a synchronization circuit for forming synchronizing signals in synchronous with the drive pulse of the foregoing second drive pulse generation circuit; and a signal processor circuit for performing image processing on the output signal from the foregoing first imaging device when the first electronic endoscope is connected and for performing image processing on the output signals of the second imaging device by inputting the synchronizing signals from the foregoing synchronization circuit.

[0011] An embodiment of the invention according to claim 2 is characterized in that the foregoing processor unit includes a determination circuit for automatically determining the type of the electronic endoscope connected to the foregoing processor unit, and the foregoing selection circuit and synchronization circuit are operated based on the determination results.

[0012] According to the foregoing configuration, at the processor unit, the type of the electronic endoscope is determined, for example, by inputting identifying information from the electronic endoscope, and when it is determined to be the first electronic endoscope, the imaging device is driven by the first drive pulse generation circuit in the processor unit, and video signals are processed with various timing

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1 signals which are formed based on the clock signal used on  
2 the first drive pulse generation circuit.

3 [0013] On the other hand, when it is determined to be the  
4 second electronic endoscope, the imaging device is driven by  
5 the second drive pulse generation circuit on the electronic  
6 endoscope, and synchronizing signals synchronized with the  
7 drive pulse of the second drive pulse generation circuit are  
8 formed. The synchronizing signals include, for example,  
9 horizontal synchronizing signals, vertical synchronizing  
10 signals, and the like, and sampling pulses of video signals  
11 and other timing signals are formed based on the synchronizing  
12 signals, and various image processing is performed.

13 [0014] In this way, the present invention allows to connect  
14 an electronic endoscope having a second imaging device with  
15 a different pixel density to the processor unit which includes  
16 the first drive pulse generation circuit to drive the first  
17 imaging device with a reference pixel density in the first  
18 electronic endoscope, and also allows to perform image  
19 processing on the signals outputted from each imaging device  
20 by a single processor unit.

21  
22 BRIEF DESCRIPTION OF THE DRAWINGS

23 [0015] FIG. 1 is a block diagram showing the circuit  
24 configuration of the electronic endoscope apparatus according

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1 to an embodiment of the present invention with the first  
2 endoscope being connected;

3 FIG. 2 is a block diagram of the electronic endoscope  
4 apparatus according to an embodiment with the second endoscope  
5 being connected; and

6 FIG. 3 is a block diagram showing a schematic configuration  
7 of a conventional electronic endoscope apparatus.

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9 DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

10 [0016] FIGS. 1 and 2 show the configuration of an  
11 electronic endoscope apparatus according to an embodiment of  
12 the present invention, and the apparatus, as shown in the  
13 figures, includes a first electronic endoscope (hereinafter  
14 referred to as endoscope) 10A and a second endoscope 10B, both  
15 of which are of a different type from one another and connectable  
16 to the processor unit 12. The first endoscope 10A in FIG.  
17 1 includes, for example, a 410-kilo-pixel CCD 14A, which will  
18 capture the image of the object to be observed through an object  
19 lens system. Furthermore, the first endoscope 10A includes  
20 a endoscope identifying information generation module 15A.  
21 In this embodiment, identifying information which is specific  
22 to each endoscope and recorded on a storage medium such as  
23 an EEPROM is sent out by communication means, and the  
24 identifying information is read out and interpreted by a  
25 microprocessor 22 on the processing unit, which will be

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1 described later. It is also possible to use a shape identifying  
2 member placed at a connector junction as the identifying  
3 information generating unit 15A.

4 [0017] The second endoscope 10B in FIG. 2 includes, for  
5 example, a 270-kilo-pixel CCD 14B and a second drive pulse  
6 generator circuit 16B to drive the CCD 14B. This drive pulse  
7 generating circuit 16B generates various drive pulses such  
8 as a horizontal pulse, a vertical pulse, and a sweep-out (SUB)  
9 pulse. The second endoscope 10B also includes a endoscope  
10 identifying information generation unit 15B with a  
11 microprocessor.

12 [0018] On the other hand, the processor unit 12 includes  
13 a first drive pulse generation circuit 16A via a switching  
14 element 18, and connection/disconnection of the first drive  
15 pulse generation circuit 16A to/from the CCD 14A of the  
16 foregoing first endoscope 10A is switched by the switching  
17 element 18. The processor unit 12 also includes a  
18 synchronization circuit 20 via a switching element 19, and  
19 connection/disconnection of this synchronization circuit 20  
20 to/from the second drive pulse generation circuit 16B of the  
21 foregoing second endoscope 10B is switched by the switching  
22 element 19.

23 [0019] Furthermore, the processor unit 12 includes a  
24 microprocessor 22 for switching control of the foregoing  
25 switching elements 18, 19 and for overall control of other

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1 parts and a signal processing circuit 23 to perform various  
2 image processing, and either the output signal of the CCD 14A  
3 of the first endoscope 10A or the output signal of the CCD  
4 14B of the second endoscope 10B is inputted to the signal  
5 processing circuit, and image processing such as correlated  
6 double sampling, amplification, gamma correction, and the like  
7 is performed for these signals.

8 [0020] The embodiment being configured as described above,  
9 when the first endoscope 10A is connected to the processor  
10 unit 12 as shown in FIG. 1, the microcomputer 22 of the processor  
11 unit 12 recognizes that the connected endoscope is the first  
12 endoscope 10A (or 410-kilo-pixel CCD 14A) from the identifying  
13 information which is received from an endoscope identifier 15A.  
14 And the microcomputer 22 disconnects the synchronization  
15 circuit 20 and connects the first drive pulse generation  
16 circuit 16A to the CCD 14A by controlling the switching elements  
17 18, 19 and activates the operation of the drive pulse generation  
18 circuit 16A.

19 [0021] In this case, based on the clock signals obtained  
20 on the oscillator of the processor unit 12, the drive pulse  
21 generation circuit 16A and the signal processing circuit 23  
22 operate to generate video signals as in a conventional manner,  
23 and video signals such as R (Red), G (Green), B (Blue), or  
24 Y (luminance)/C (Color) are outputted to the monitor from this  
25 signal processing circuit 23.

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1 [0022] On the other hand, as shown in FIG. 2, when the  
2 second endoscope 10B is connected to the processor unit 12,  
3 the foregoing microcomputer 22 recognizes that the connected  
4 endoscope is the second endoscope 10B (or 170- kilo-pixel CCD  
5 14B) from the identifying information which is received from  
6 a endoscope identifier 15B and disconnects the first drive  
7 pulse generation circuit 16A and connects the synchronization  
8 circuit 20 to the second drive pulse generation circuit 16B  
9 by switching the switching elements 18, 19.

10 [0023] In this case, in the second endoscope 10B, the  
11 second drive pulse generation circuit 16B generates horizontal  
12 drive pulses, vertical drive pulses, sweep-out pulses, and  
13 the like based on the clock signal of the oscillator on the  
14 endoscope, and image signals are read out with these drive  
15 pulses from the CCD 14B, and these signals are supplied to  
16 the signal processing circuit 23. Also, from the foregoing  
17 second drive pulse generation circuit 16B, the foregoing  
18 horizontal drive pulse and the vertical drive pulse (or clock  
19 signal) are supplied to the synchronization circuit 20 and,  
20 at this synchronization circuit 20, horizontal synchronizing  
21 signals, vertical synchronizing signals, and other  
22 synchronizing signals are generated based on the foregoing  
23 signals and outputted to the signal processing circuit 23.

24 [0024] Therefore, in this signal processing circuit 23,  
25 sampling pulses and other timing signals for other signal

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1 processing are formed from the foregoing synchronizing signals,  
2 and various image processing are to be performed with these  
3 signals, and the image of the object to be observed will be  
4 displayed on the monitor with the video signals outputted from  
5 the signal processing circuit 23.

6 [0025] Although the second endoscope 10B has been  
7 described as one with a 170-kilo-pixel CCD 14B in the foregoing  
8 embodiment, but a high resolution CCD with more than 410  
9 kilo-pixels or a CCD with pixel density conforming to a  
10 television standard other than NTSC may be used as the CCD  
11 14B.

12 [0026] As described so far, in the embodiment, an  
13 electronic endoscope 10B having a CCD 14B with a different  
14 pixel density includes a drive pulse generation circuit 15B,  
15 and the processor unit 12 includes switching elements 18, 19  
16 for the drive pulse generation circuit and is configured to  
17 generate signals synchronous with the signals used at other  
18 electronic endoscopes, thus allowing to readily connect a  
19 plurality of CCDs with different pixel densities by adding  
20 only a simple configuration to the processor unit 12.

21 [0027] As explained so far, according to the present  
22 invention, a second endoscope, which have a second imaging  
23 device and a second pulse generation circuit, is configured  
24 to be connectable to the processor unit which has the first  
25 drive pulse generation circuit to drive the first imaging

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1 device in the first electronic endoscope, and thus the video  
2 signal can be formed by the foregoing second imaging device  
3 as well, and therefore, a single processor unit will suffice  
4 even when using an electronic endoscope employing a CCD with  
5 a different pixel density and thus an electronic endoscope  
6 apparatus with minimized waste in terms of configuration and  
7 cost is achieved.

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